

# NON CONTACT TONOMETRY: A FLUID STRUCTURE INTERACTION STUDY

E. Redaelli<sup>1</sup>, B. Fantaci<sup>1</sup>, J. F. Rodriguez<sup>2</sup>, G. Luraghi<sup>2</sup>, J. Grasa<sup>1</sup>

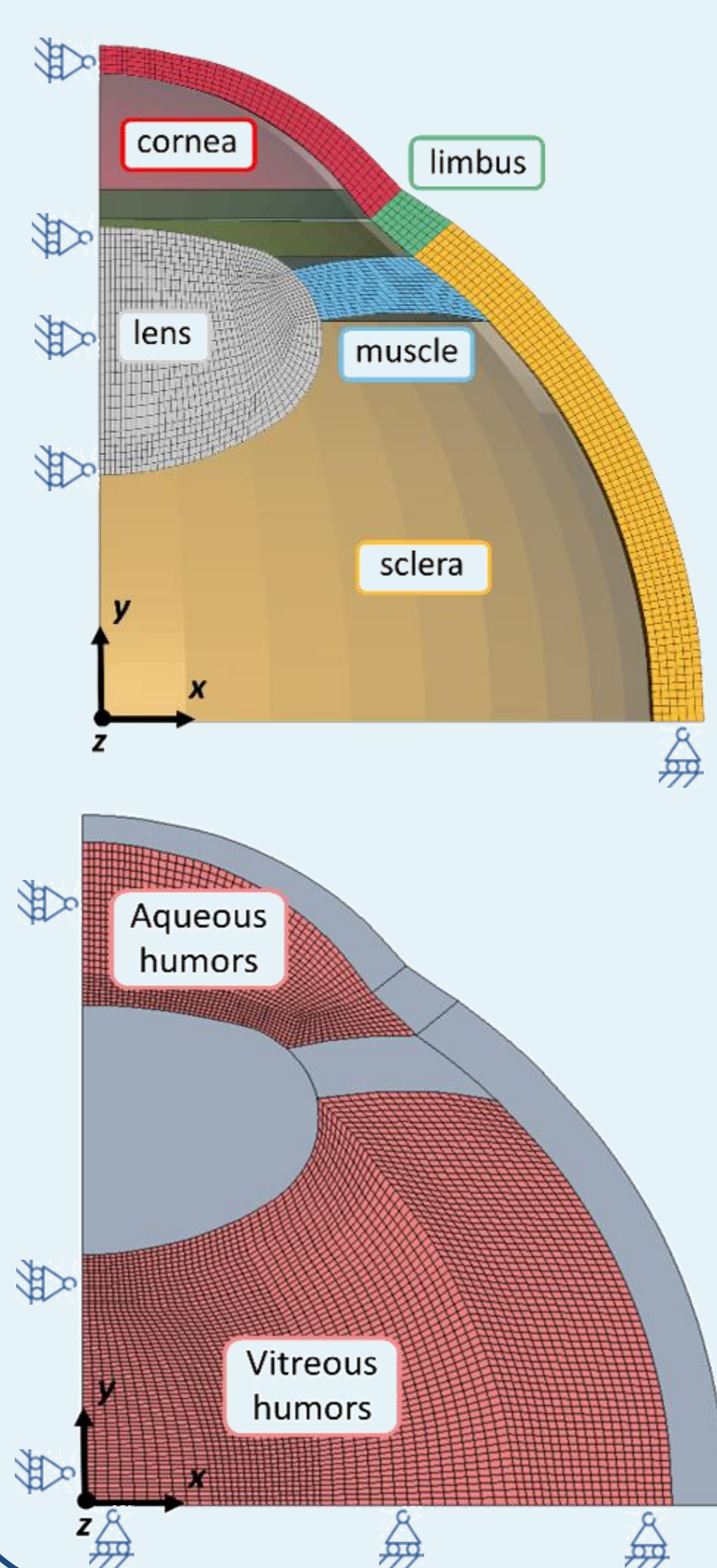
1. AMB Group. Aragón Institute of Engineering Research (I3A), University of Zaragoza, Spain  
 2. Politecnico di Milano, Italy

## INTRODUCTION

The cornea is the primary refractive surface of the eye, responsible for approximately  $\frac{2}{3}$  of its optical power [1]. The corneal shape is the result of the equilibrium between its **mechanical stiffness**, **intraocular pressure (IOP)**, and the **external forces** acting upon it. An imbalance between these parameters can produce ocular pathologies which seriously affect patient sight. The Non Contact Tonometry (*Corvis-ST*) is a diagnostic tool that aims at determining the IOP and characterizing the mechanical properties of the corneal tissue by applying a **short high velocity air-jet** to the tissue. A deeper understanding of the process is required to **translate the results of the test into clinical data**. From a modelling perspective, the best numerical approach to reproduce the procedure is the Fluid Structure Interaction (**FSI**) modelling [3]. This work presents a FSI analysis to virtually apply an air-jet to a 3D idealized eye model.

## METHODS

### Eye model



### Material Model

**Cornea and Limbus:** anisotropic hyperelastic material.

Cornea: two families of fibers perpendicular to each other.

Limbo: one circumferential family of fibers.

Isotropic Demiray formulation.

Anisotropic Holzapfel-Gasser-Ogden formulation.

$$\Psi = D_1[\exp\{D_2(\bar{I}_1 - 3)\} - 1] + \frac{k_1}{2k_2}[\exp\{k_2(\bar{I}_4 - 1)\} - 1] + \frac{k_3}{2k_4}[\exp\{k_4(\bar{I}_6 - 1)\} - 1] + \frac{\kappa}{2}(J - 1)^2$$

$$D_1 = 2.77 \cdot 10^{-4} \text{ MPa}$$

$$k_1 = 0.0208 \text{ MPa}$$

$$k_3 = 0.0208 \text{ MPa}$$

$$D_2 = 120.6 [-]$$

$$k_2 = 516.9 [-]$$

$$k_4 = 516.9 [-]$$

$$\kappa = 334.04 \text{ MPa}$$

**Sclera:** Hyperelastic material: Yeoh model.

$$\Psi = C_{10}(\bar{I}_1 - 3) + C_{20}(\bar{I}_1 - 3)^2 + C_{30}(\bar{I}_1 - 3)^3 + \frac{\kappa}{2}(J - 1)^2$$

$$C_{10} = 0.81 \text{ MPa}$$

$$C_{20} = 54.05 \text{ MPa}$$

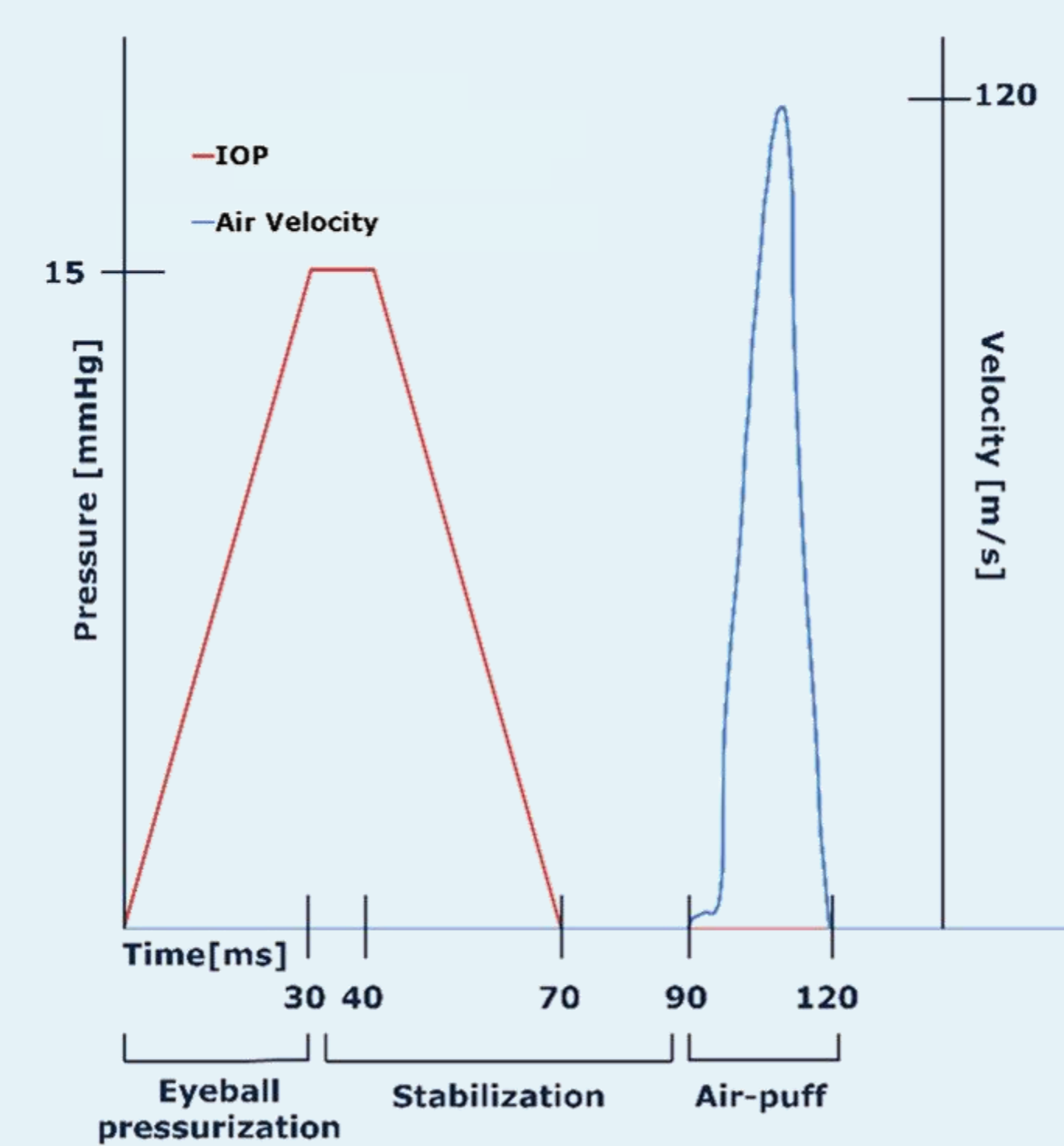
$$C_{30} = 2332.26 \text{ MPa}$$

**Lens and Muscle:** linear elastic material.

**Humors:** Newtonian fluids.

**Air:** incompressible fluid.

### Boundary conditions



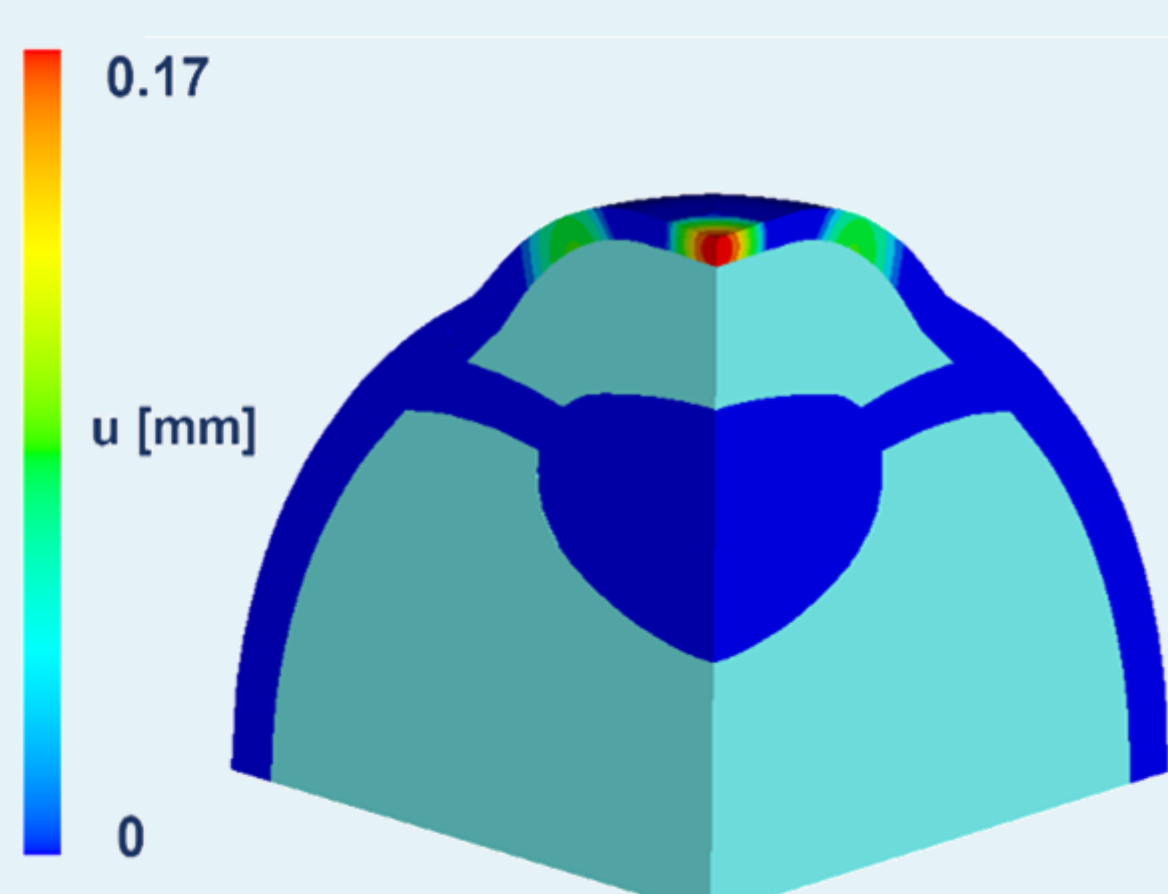
- Zero pressure is imposed as the outflow condition.

## RESULTS

The Non Contact Tonometry monitors the bidirectional deformation of the cornea through two applanation points during loading (the cornea deforms inwardly) and unloading[1].

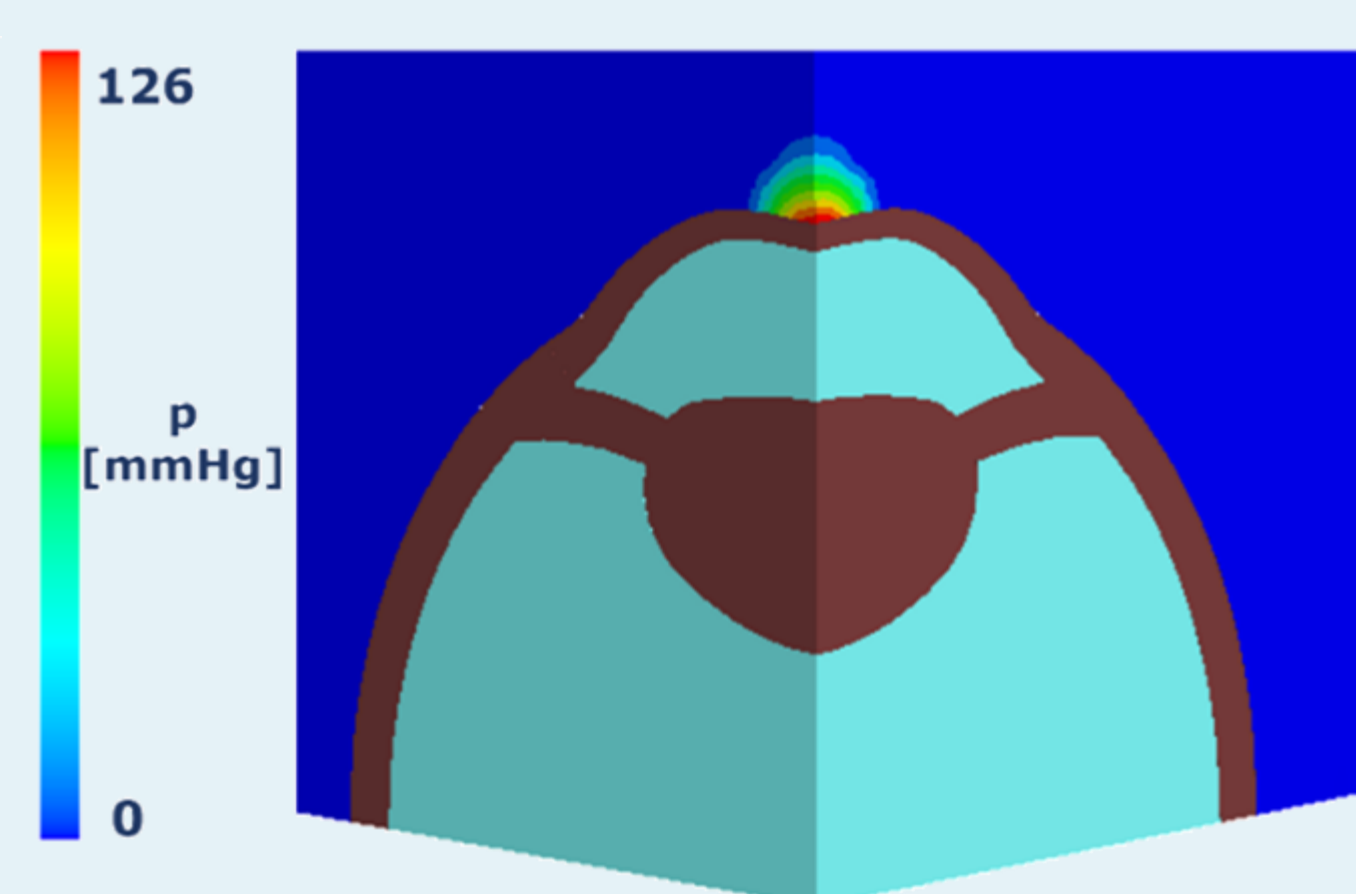
### Corneal deformation

@maximum deformation point



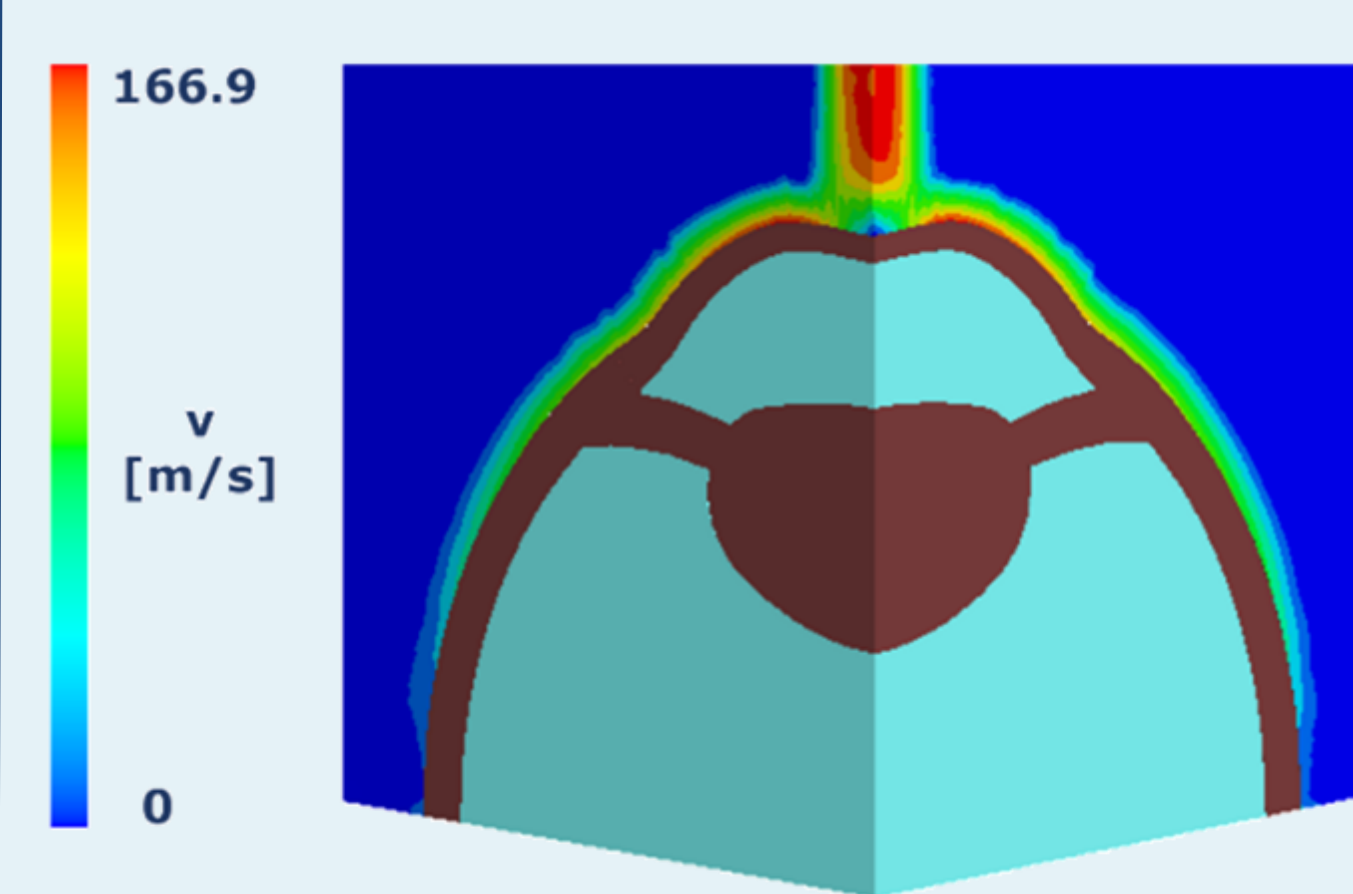
### Pressure

@maximum deformation point

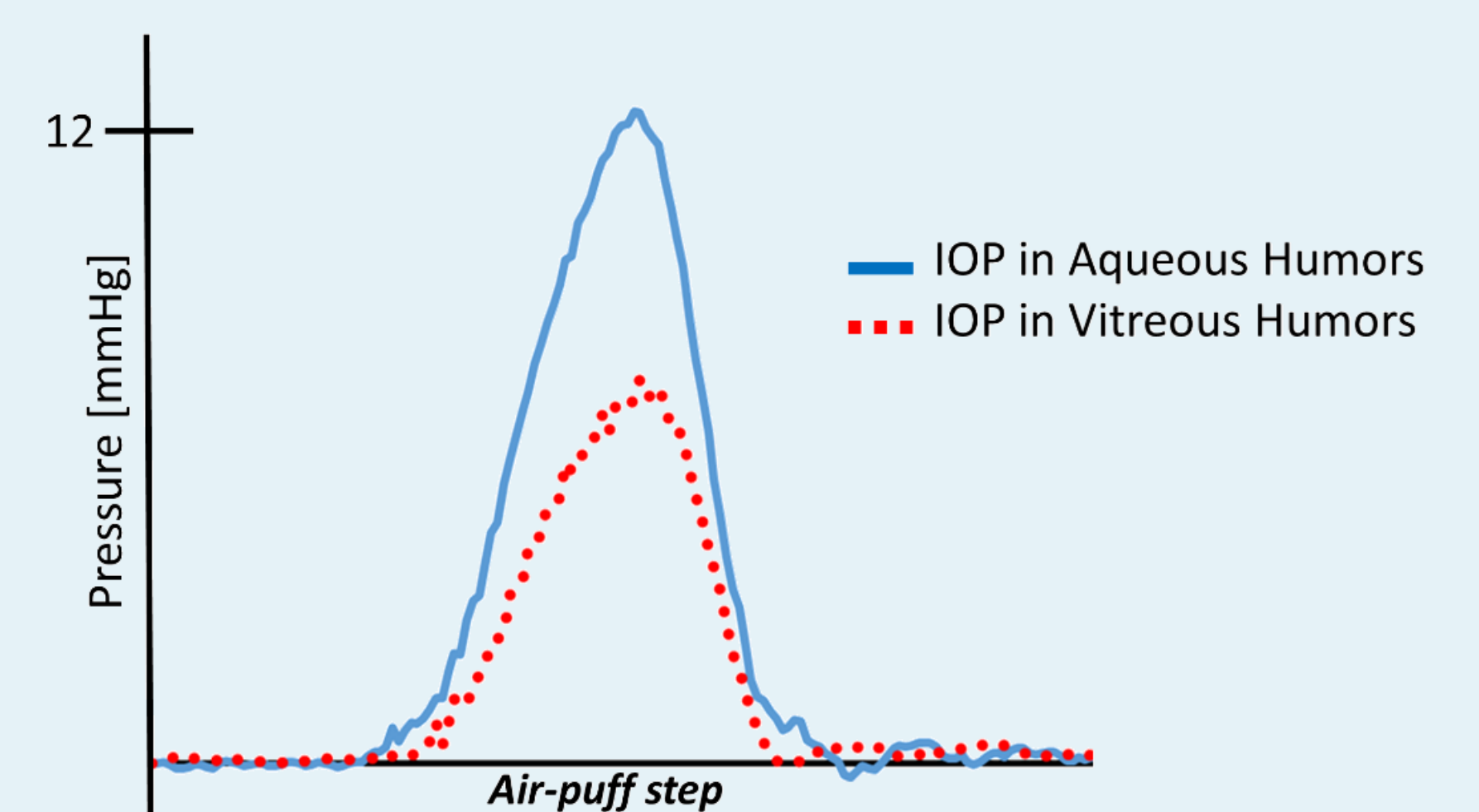


### Velocity

@maximum deformation point



### Intraocular pressure during the test



## CONCLUSIONS

The development of a strong FSI tool amenable to model coupled structures and fluid can be useful to **correlate the results of the Non Contact Tonometry test to the biomechanical properties of the cornea**. With the proposed simulation, it is possible to **vary the mechanical stiffness of each tissue** of the eye studying the influence that each parameter has on the results of the test. Moreover, the eye can be modelled with **different intraocular pressures** in order to study the effect of the IOP on the Non Contact Tonometry. In a second step, the properties of the corneal tissue can be determined through an **optimisation process** by numerically reproducing the deformation of the cornea.

## REFERENCES

- 1) CHONG, J.; DUPPS JR, W. J. Corneal biomechanics: Measurement and structural correlations. *Experimental Eye Research*, 2021, vol. 205, p. 108508.
- 2) ARIZA-GRACIA, M. A., et al. Automatized patient-specific methodology for numerical determination of biomechanical corneal response. *Annals of biomedical engineering*, 2016, vol. 44, no 5, p. 1753-1772.
- 3) ARIZA-GRACIA, M. A., et al. Fluid-structure simulation of a general non-contact tonometry. A required complexity?. *Computer methods in applied mechanics and engineering*, 2018, vol. 340, p. 202-215.