

INFLUENCE OF MECHANICAL PROPERTIES ON PHOTOREFRACTIVE KERATECTOMY OUTCOME

B. Fantaci¹, M. A. Ariza-Gracia³, I. Cabeza-Gil¹, J. Grasa^{1,2}, B. Calvo^{1,2}

1. Aragón Institute of Engineering Research (I3A), University of Zaragoza, Spain.

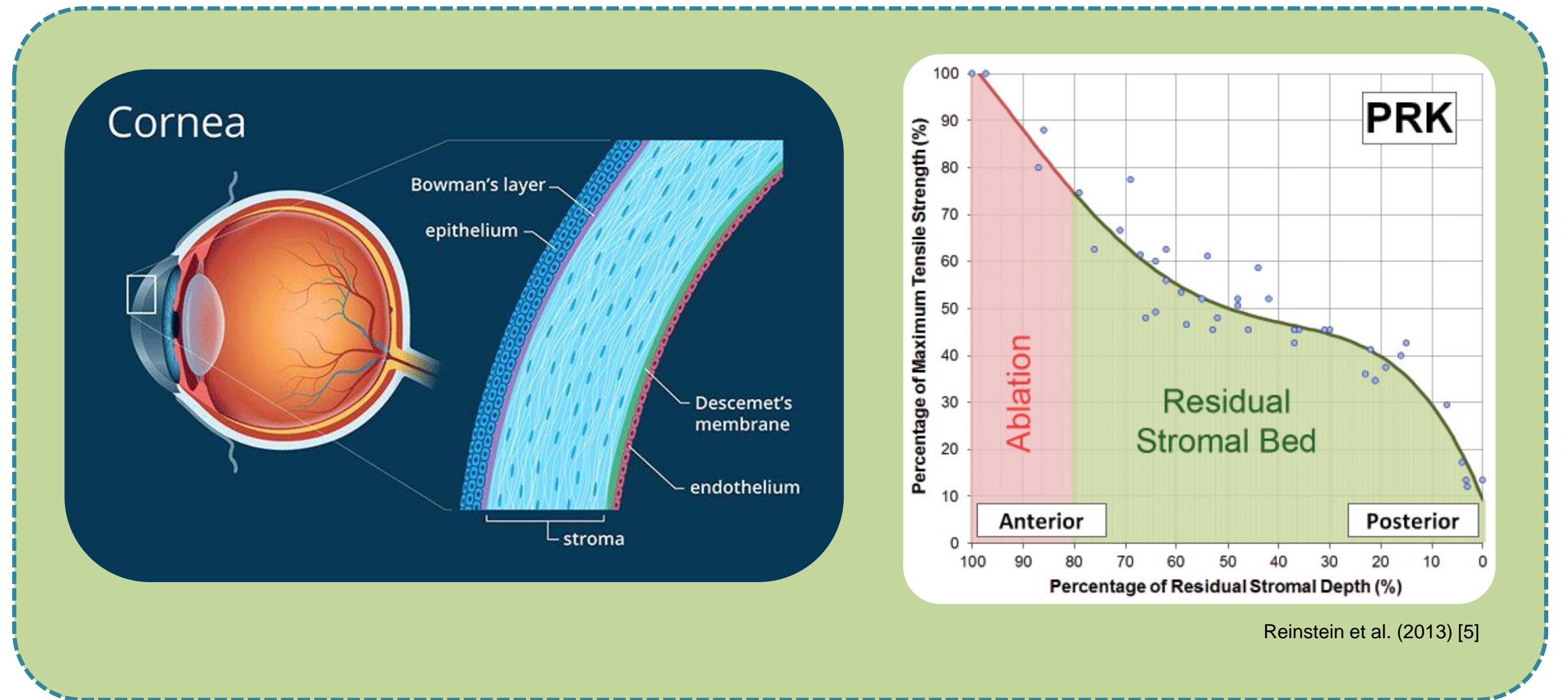
2. CIBBER-BBN. Bioengineering, Biomaterials and Nanomedicine Networking Biomedical Research Center, Spain.

3. ARTORG. University of Bern, Switzerland.

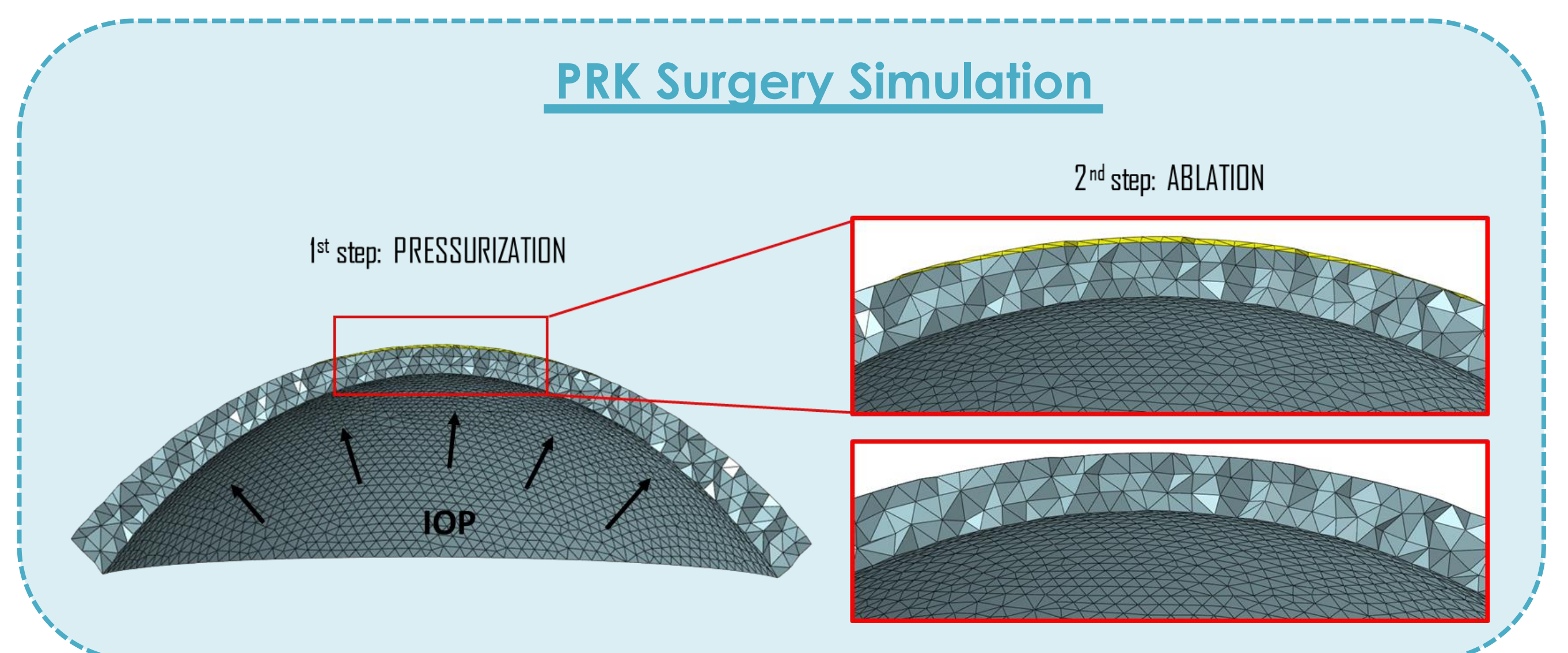
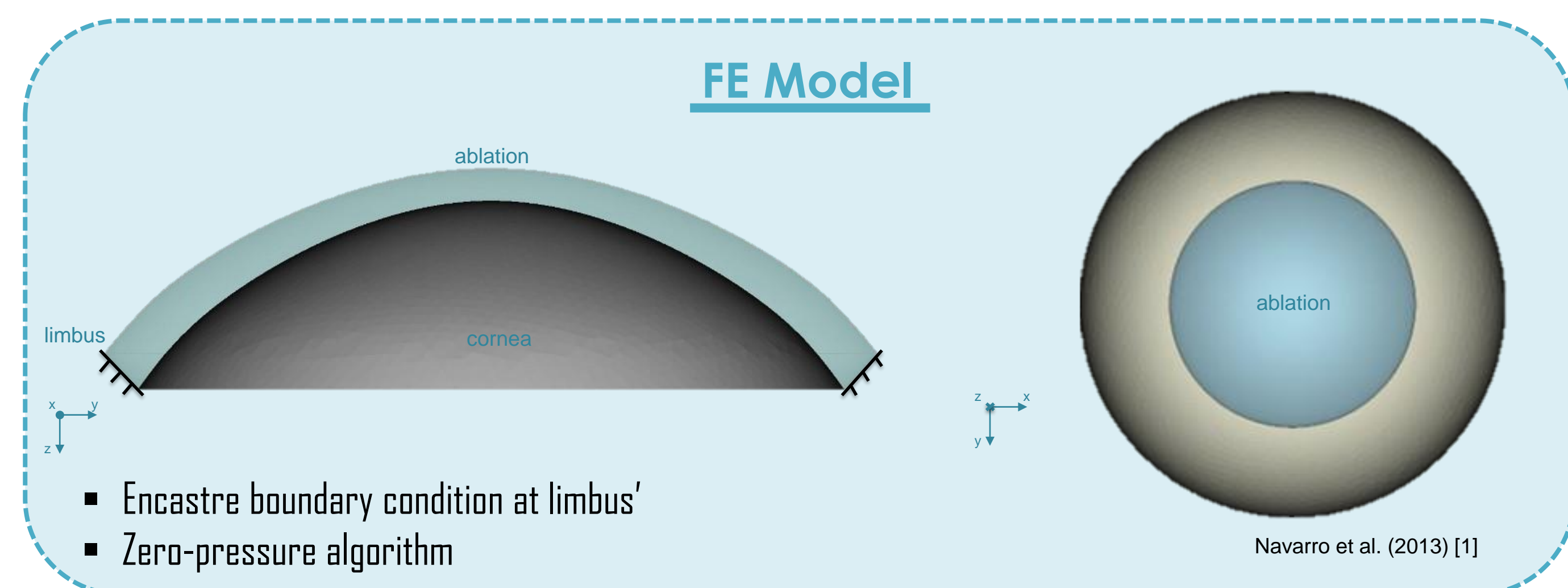


INTRODUCTION

- Laser refractive surgeries are widely used in correction of vision defects such as **myopia** and **astigmatism**.
- **Photorefractive Keratectomy (PRK)** consists of reshaping the anterior corneal surface with a laser, by following an ablation profile [2], in order to achieve the spectacle independence (**desired diopters correction**).
- The removal of the ablation tissue affects the **biomechanics** of the cornea, causing deformations and stresses on the tissue, due to the action of the intraocular pressure (**IOP**) inside the eye cavity.
- In this work, a **FE model** of the cornea has been developed to address the influence of geometrical, physiological and material parameters on the final outcome of PRK surgery simulation.



MATERIALS AND METHODS



Material Model

Strain energy density function $\psi = \psi^{\text{matrix}}(\bar{I}_1, J) + \sum_{i=4,6} \psi^{\text{fibers}}(C_{\text{dis}}, H_i)$

Isotropic Neo-Hookean term + Volumetric term $\psi^m = C_{10}(\bar{I}_1 - 3) + \frac{1}{D}(\ln J)^2$

Anisotropic Halzapfel-Gasser-Odgen term [1]

$\psi^f = \frac{k_1}{2k_2}(e^{k_2(\bar{I}_i - 1)^2} - 1)$ for $i=4,6$ where

$\bar{I}_1 = \text{tr}(H_1 C_{\text{dis}}) = 2k_{\text{ip}}k_{\text{op}}\bar{I}_1 + 2k_{\text{op}}(1 - 2k_{\text{ip}})\bar{I}_i + (1 - 6k_{\text{ip}}k_{\text{op}} - 2k_{\text{op}}(1 - 2k_{\text{ip}}))\bar{I}_n$

k_{ip} : in-plane dispersion $\in [0,1,0,5]$
 k_{op} : out-of-plane dispersion $\in [1/3, 0,5]$

C_{10} [kPa]	k_1 [kPa]	k_2 [-]	D [kPa ⁻¹]
30	20	400	0,0003636

Wang et al. (2021) [2]

Statistical analysis

2⁵ full factorial design

	C_{10} [kPa]	k_1 [kPa]	k_2 [-]	IOP [mmHg]	Thickness [μm]
Min	15	10	200	13	490
Max	45	30	600	18	550

Simulations' outcomes considered:

- diopters corrected
- apex displacement of anterior corneal surface

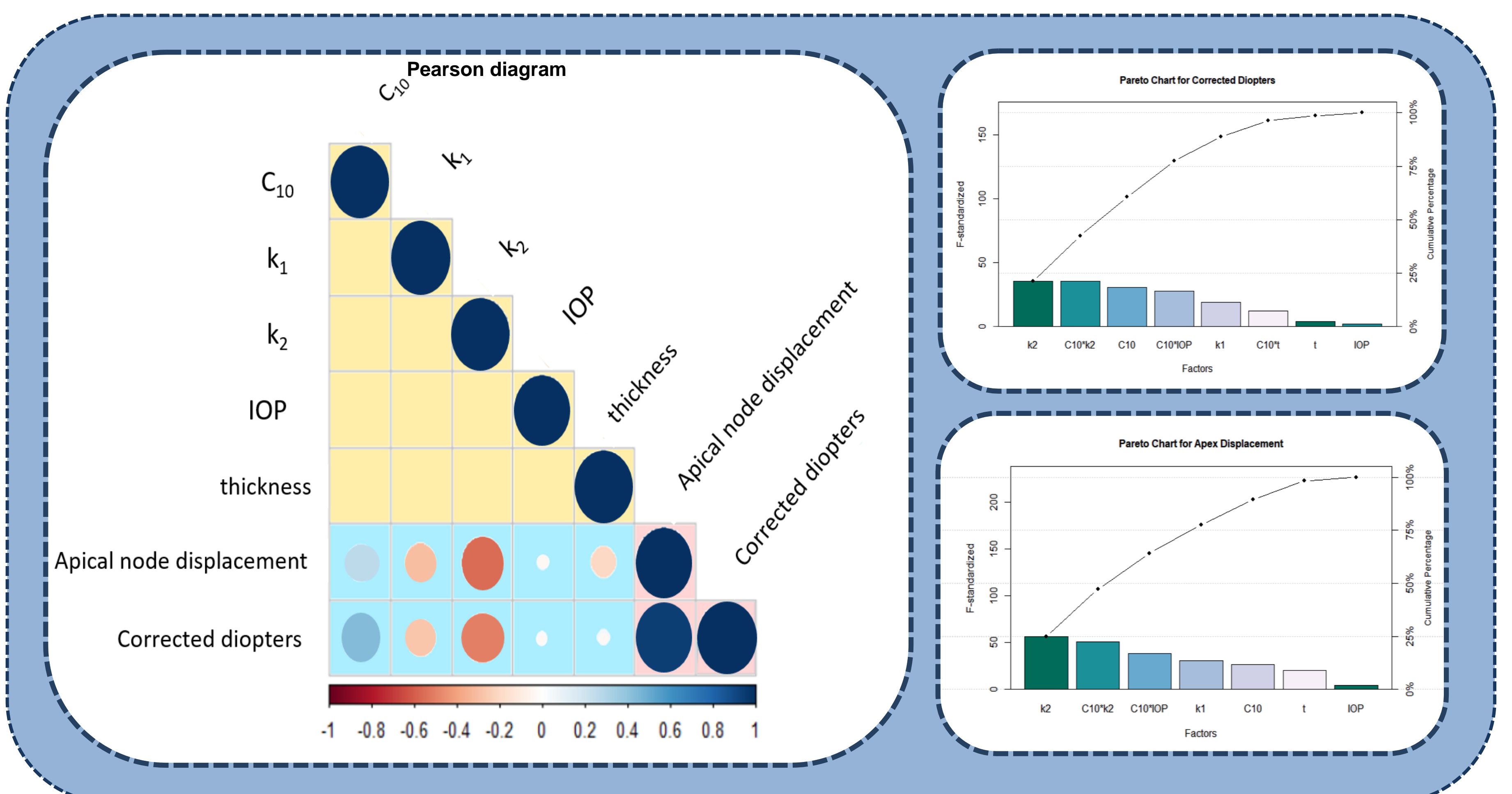
32 simulations to be analyzed

ANOVA statistical analysis



RESULTS

- The **constant k_2** turned out to be the **most influential factor**:
 - highly **non-linear contribution** of the anisotropic component of the material.
 - need of incorporating the collagen fibers when modeling the corneal tissue [2].
- **High influence** of C_{10} (isotropic contribution) and k_1 (fibers' stiffness).
- **Lower effect** of the IOP and the corneal thickness with respect to the other parameters.
- Also the **interaction** among the parameters was taken into account.



CONCLUSIONS

- In general, the material constants and their interactions have shown the major influence in determining the behavior of the corneal model.
- It is of major importance to set the proper material constants in order to perform a reliable PRK simulation, having as final goal the post-surgical optical quality of the patient.
- To achieve this goal, post-surgery mechanical deformations cannot be neglected.

REFERENCES

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