



# In vivo Mechanical Characterization of Ascending Aortas from Magnetic Resonance Imaging

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# INTRODUCTION

The rupture of ascending aortic aneurysm (AAA) results in the death of the patient in the vast majority of the cases [1]. Therefore, a proper follow-up could prevent risks. Studies suggest that mechanical properties could become useful criteria for clinical intervention [2]. In this work, we present a methodology to obtain the non-linear anisotropic properties of the AAA from magnetic resonance imaging (MRI).

## **MATERIAL & METHODS**

#### 1<sup>st</sup> Data Processing

MRI data were derived from patients who underwent surgical repair of AAA at the *Vall d'Hebron Hospital*. We segment the diastolic aorta and estimate the relative displacements between diastole and systole ( $u_{diast \to syst}$ ).

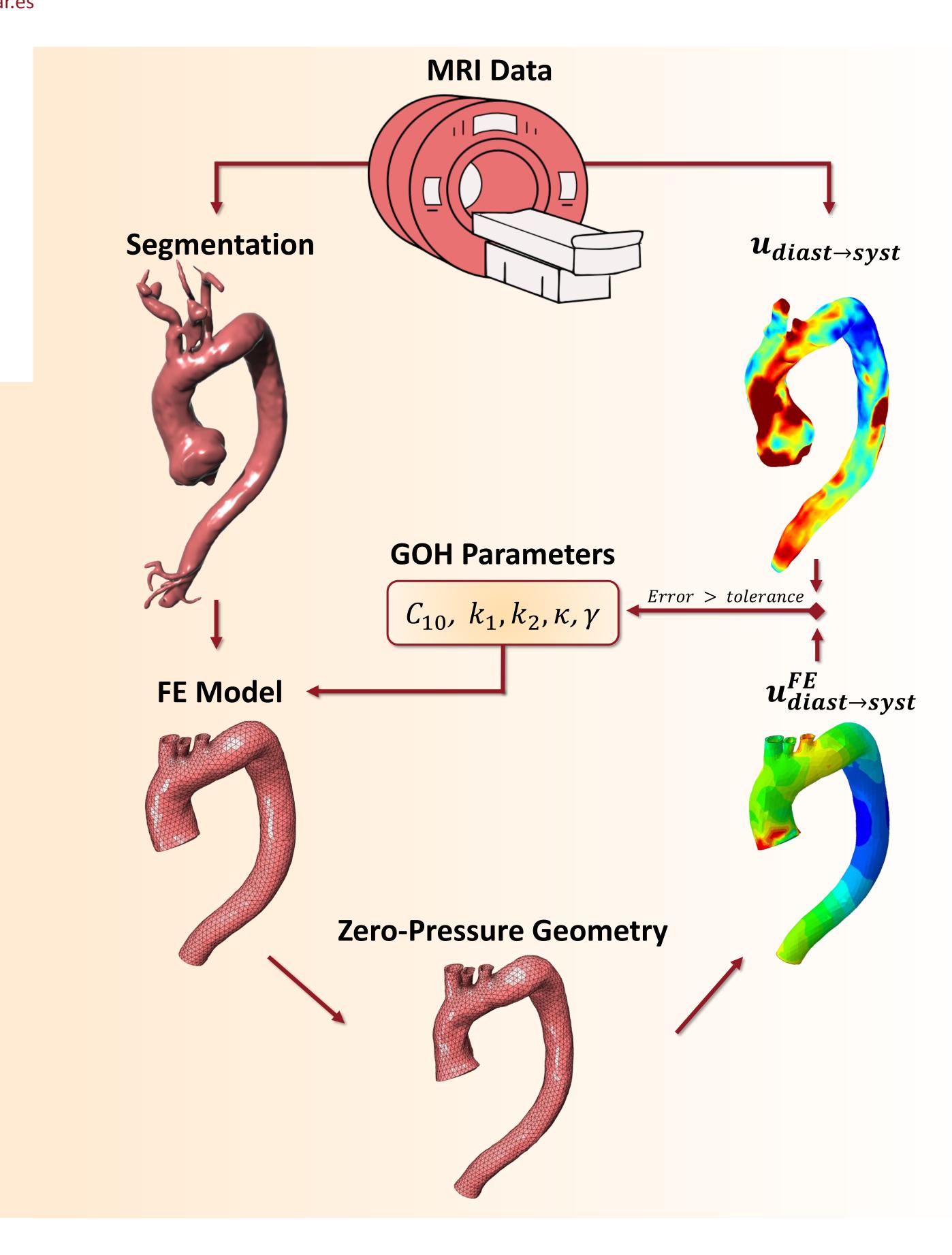
#### 2<sup>nd</sup> Finite Element (FE) Model

We assumed a thickness of 2 mm to obtain the aortic wall. Robin conditions were applied to mimic the external tissue support [3], and the measured displacements were enforced as boundary conditions to consider the heart movements.

#### 3<sup>rd</sup> Mechanical Characterization

**Longitudinal Direction** 

We implemented a pattern-search algorithm to minimize the error between the measured displacements and those derived from the FE simulation  $(u_{diast \to syst}^{FE})$ . On each iteration, a different set of material parameters from GOH strain density function was evaluated [4], and we estimated the unpressurized configuration to consider the non-linear properties.



# RESULTS In Silico Models Homogeneous Models Isotropic Longitudinal Circumferential 200 1.2 1.1 1.2 1.1 1.2 Heterogeneous Models In Vivo Displacement In vivo .vs. Optimized $\lambda$ [-] Mechanical Response In vivo .vs. in vitro Biaxial test Circumferential Direction In Silico / In Vitro data

**Optimization Results** 

1.1

## CONCLUSIONS

We have developed a methodology for extracting the nonlinear anisotropic properties and the unpressurized geometry of the ascending aortas from MRI data. Utilizing *in silico* models, we tested this methodology with many different mechanical behaviors of healthy and diseased aortas. Directly applying this characterization process to *in vivo* data yielded strong correlations with *in vitro* tests. This approach allows estimation of the stress distribution in the aortic wall and, therefore, the risk of rupture.

# **BIBLIOGRAPHY**

- 1. MELO, R.G., et al. Incidence and prevalence of thoracic aortic aneurysms: A systematic review and meta-analysis of population-based studies. Seminars in Thoracic and Cardiovascular Surgery 34, pp. 1–16 (2022) doi: 10.1053/j.semtcvs.2021.02.029
- 2. ELEFTERIADES, J.A. and FARKAS, E.A.: Thoracic aortic aneurysm. Journal of the American College of Cardiology 55(9), pp. 841–857 (2010) doi: 10.1016/j.jacc.2009.08.084
- 3. MOIREAU, P. et al. External tissue support and fluid-structure simulation in blood flows. Biomechanics and Modeling in Mechanobiology 11, pp. 1–18 (2012) doi: 10.1007/s10237-011-0289-z
- 4. GASSER, T.C., OGDEN, R.W. and HOLZAPFEL, G.A. Hyperelastic modelling of arterial layers with distributed collagen fibre orientations. Journal of The Royal Society Interface. 3(6), pp. 15-35. (2006) doi: 10.1098/rsif.2005.0073

