

# A new procedure to estimate patient-specific intraocular pressure

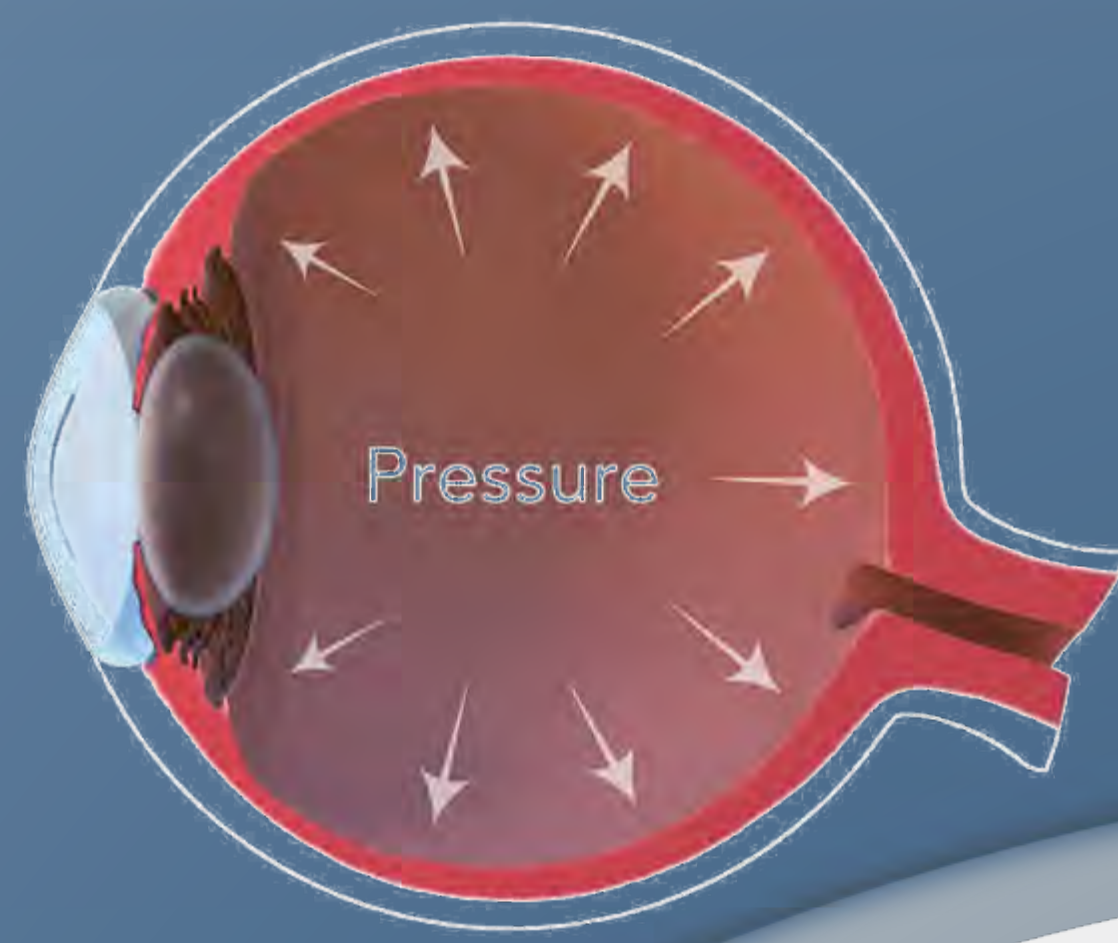
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## Intraocular Pressure

The intraocular pressure (**IOP**) is defined as the pressure inside the eye that is maintained by the balance of aqueous humor production and drainage.

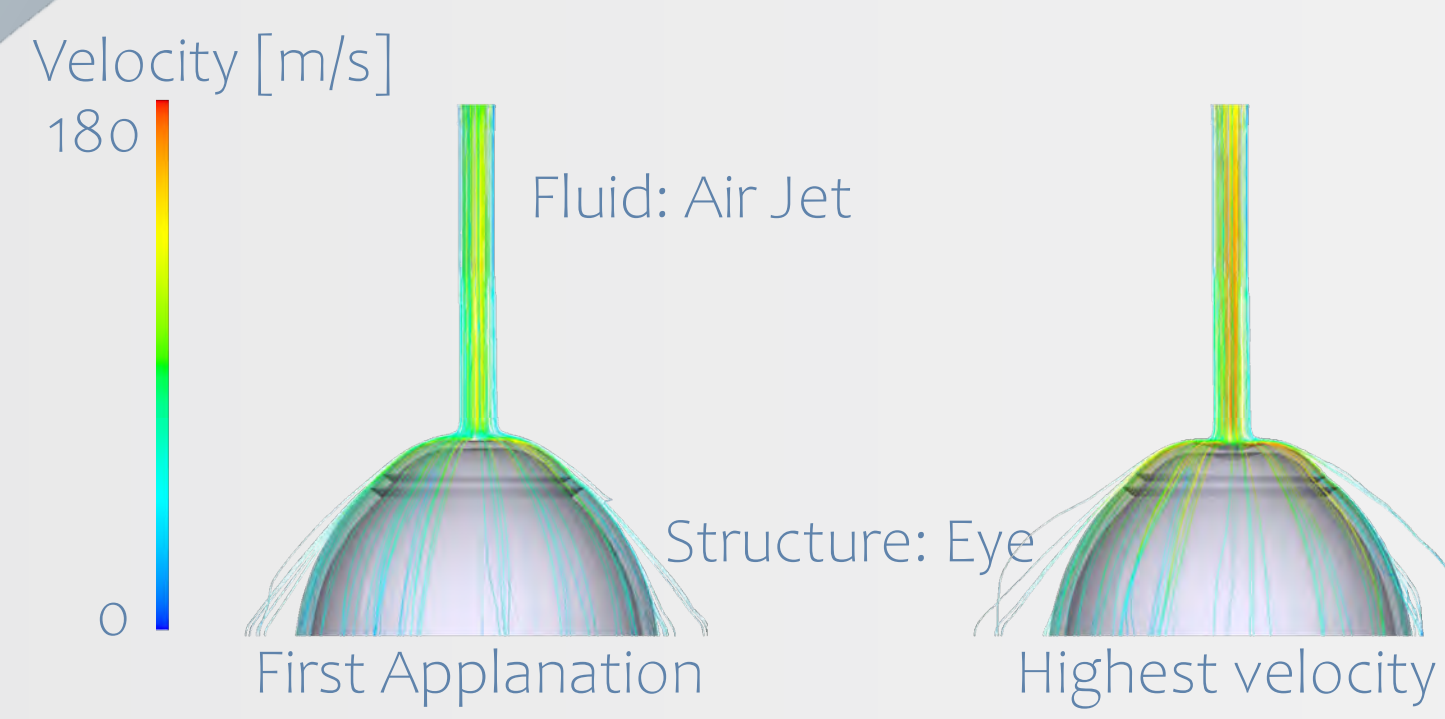
Elevated IOP is a significant risk factor for **glaucoma**, which is a leading cause of blindness worldwide.

Accurate and repeatable IOP **measurements** are the key to **diagnose** the pathology in time and to provide for effective **treatment strategies**.

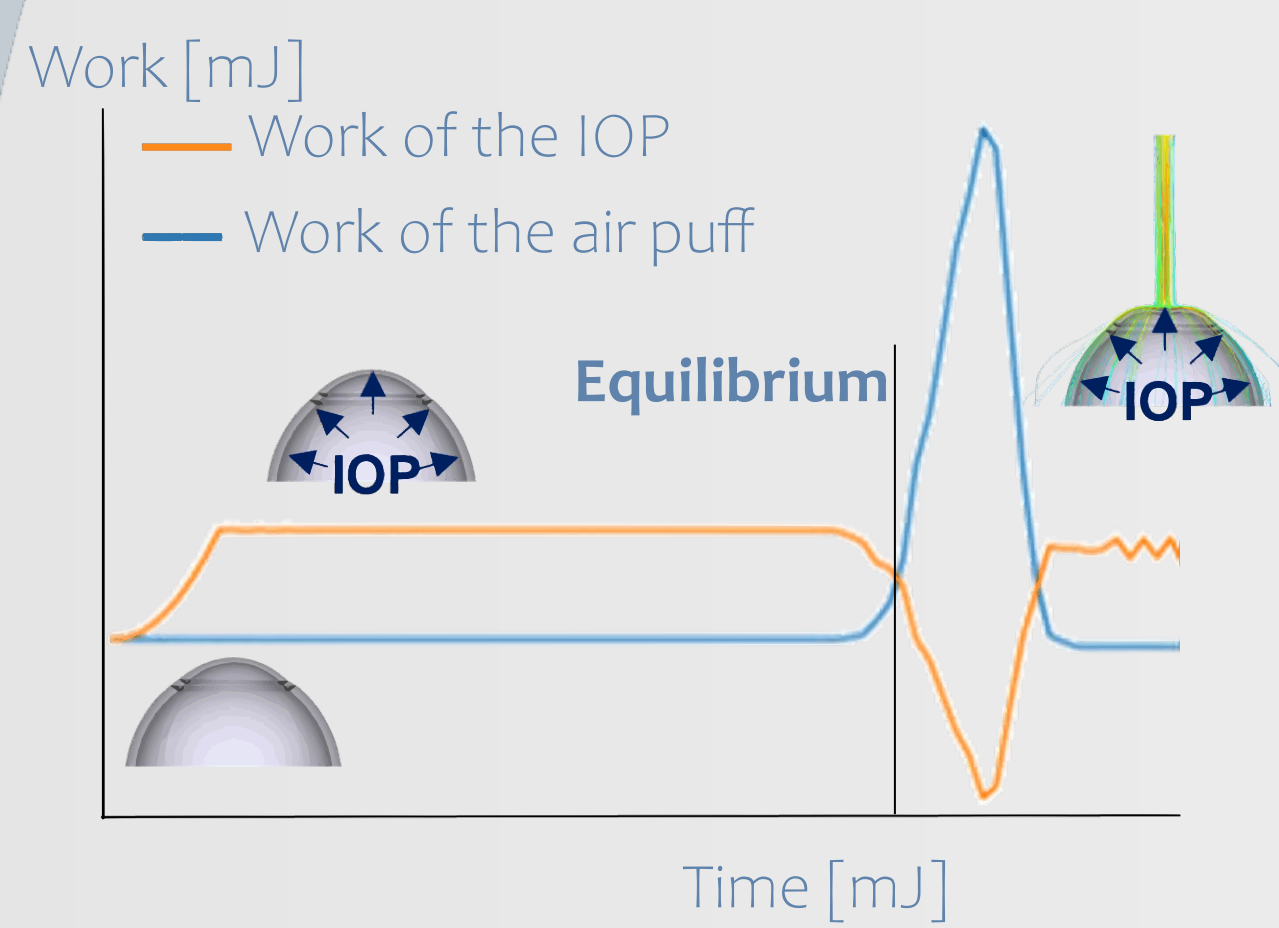


## NUMERICAL ANALYSIS

### FSI simulation



The **equilibrium** occurs when the work of the air puff and the work of the IOP on the corneal anterior surface are equal.



Changing both the **mechanical properties** of the corneal tissue and the **thickness** of the eye, the equilibrium point does not change, it only depends on the IOP.

### Working Hypothesis

	Pressurization	Equilibrium	Highest concavity
Work	$Work_{IOP} > Work_{AIR}$	$Work_{IOP} = Work_{AIR}$	$Work_{IOP} < Work_{AIR}$
Potential Energy	Maximum	Zero	Minimum
Kinetic Energy	Zero	Maximum	Zero

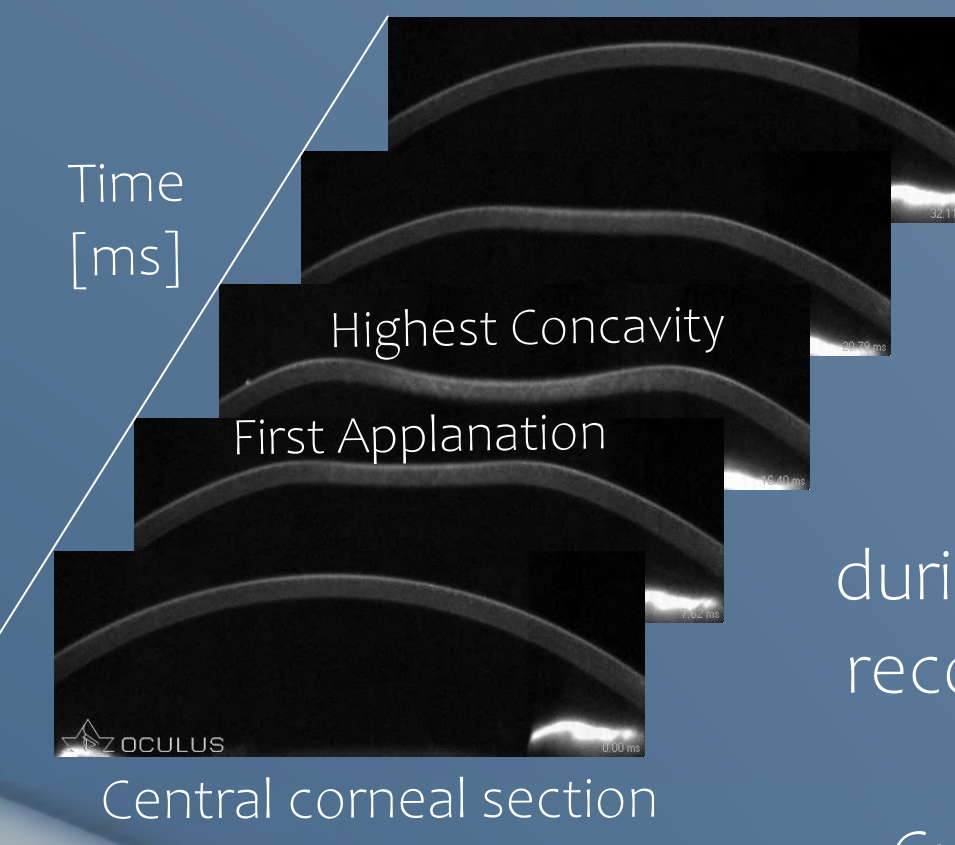
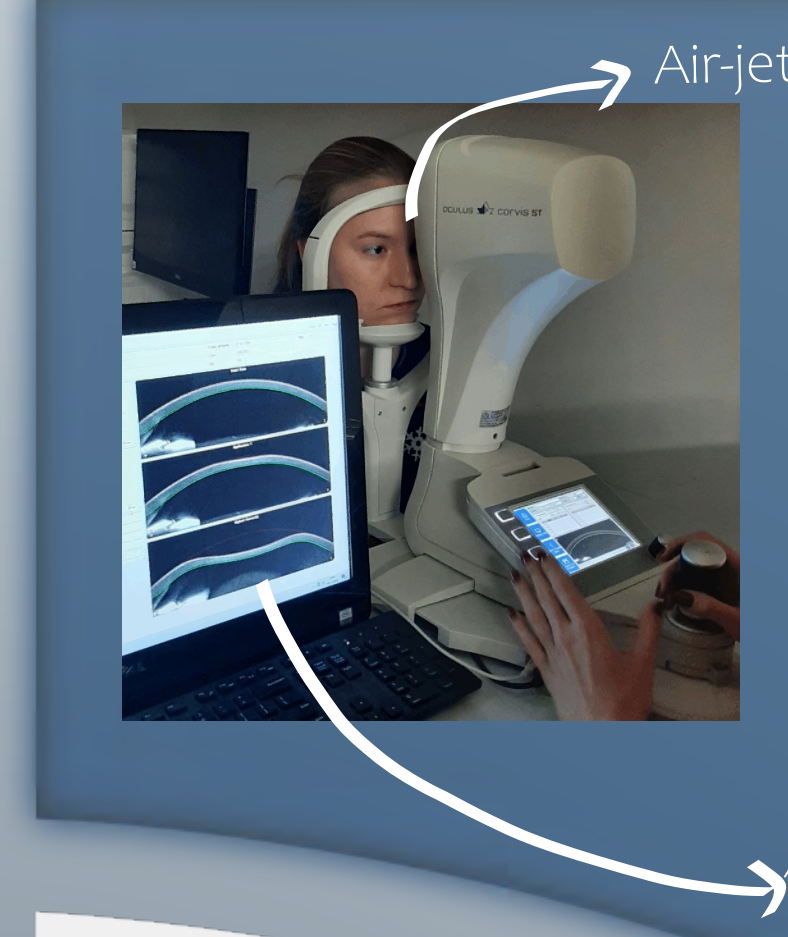
## Non Contact Tonometry

**Corvis ST** is a commercially available Non-Contact Tonometer.

An **air jet** deforms the cornea during 30 ms and the deformation is recorded by a **Scheimpflug camera**.

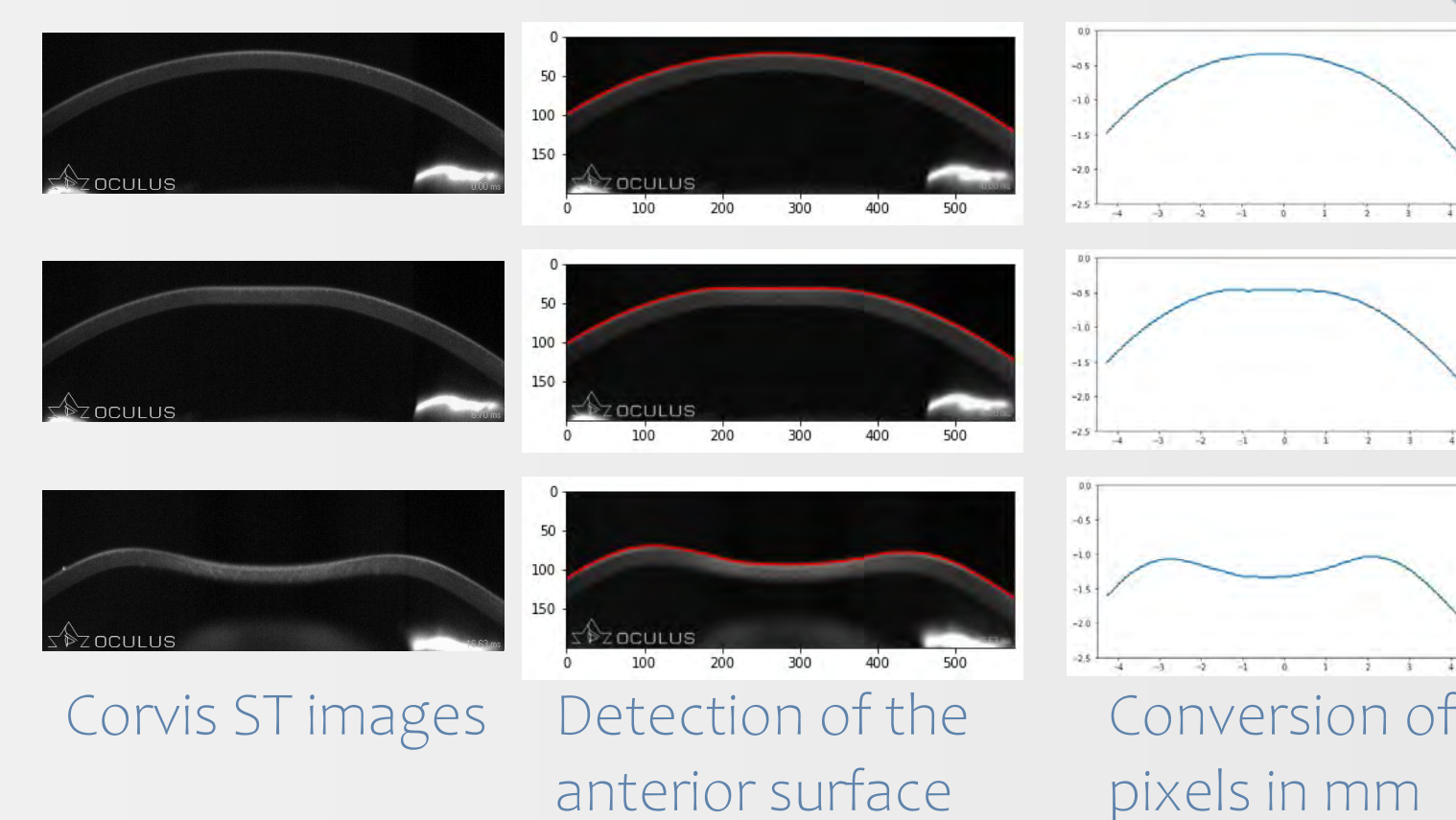
Currently, the IOP measurement is based on the **first applanation time**.

However, the applanation time also depends on the **thickness** of the cornea and on the **mechanical properties** of the corneal tissue.

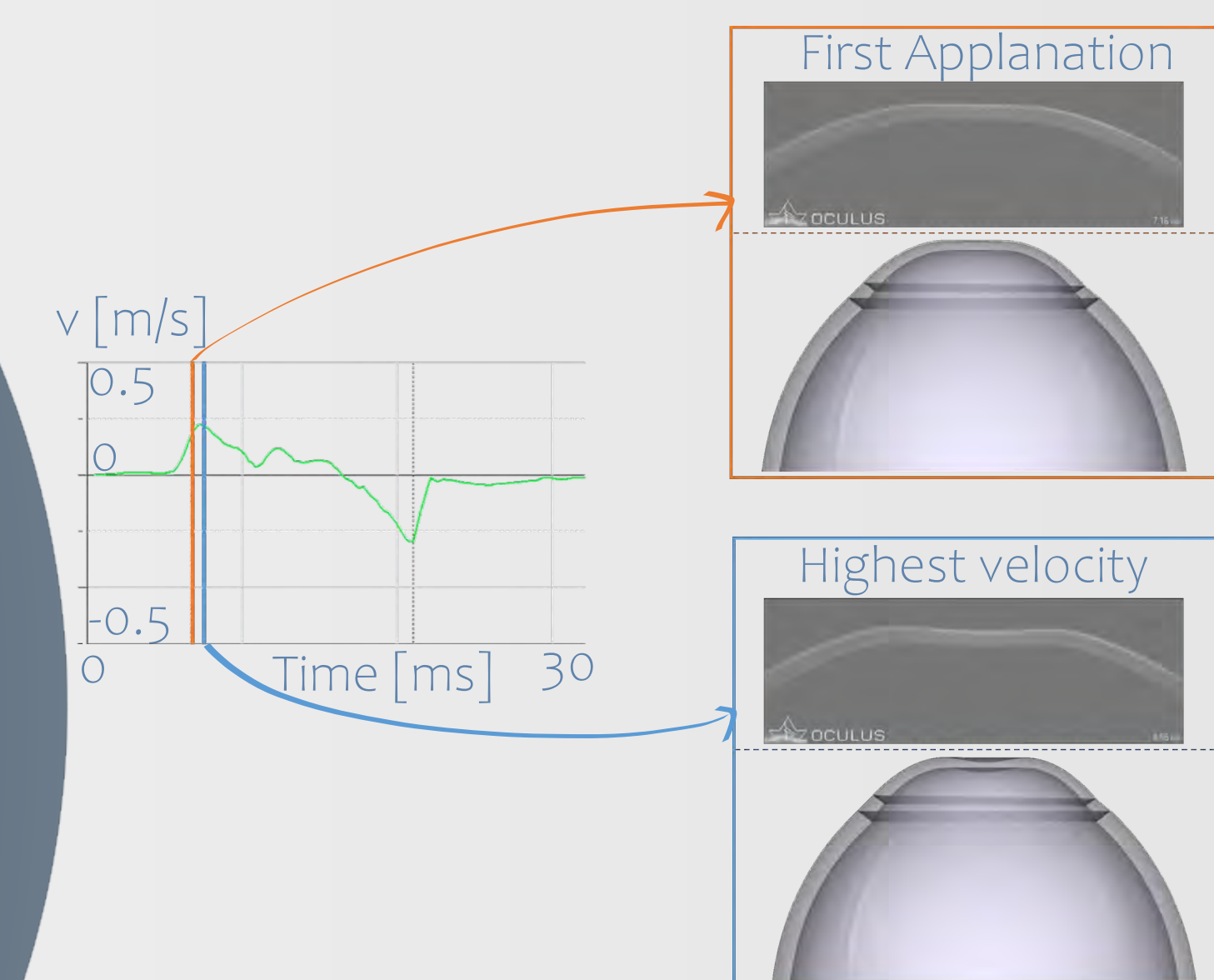


## CLINICAL ANALYSIS

### Clinical images segmentation

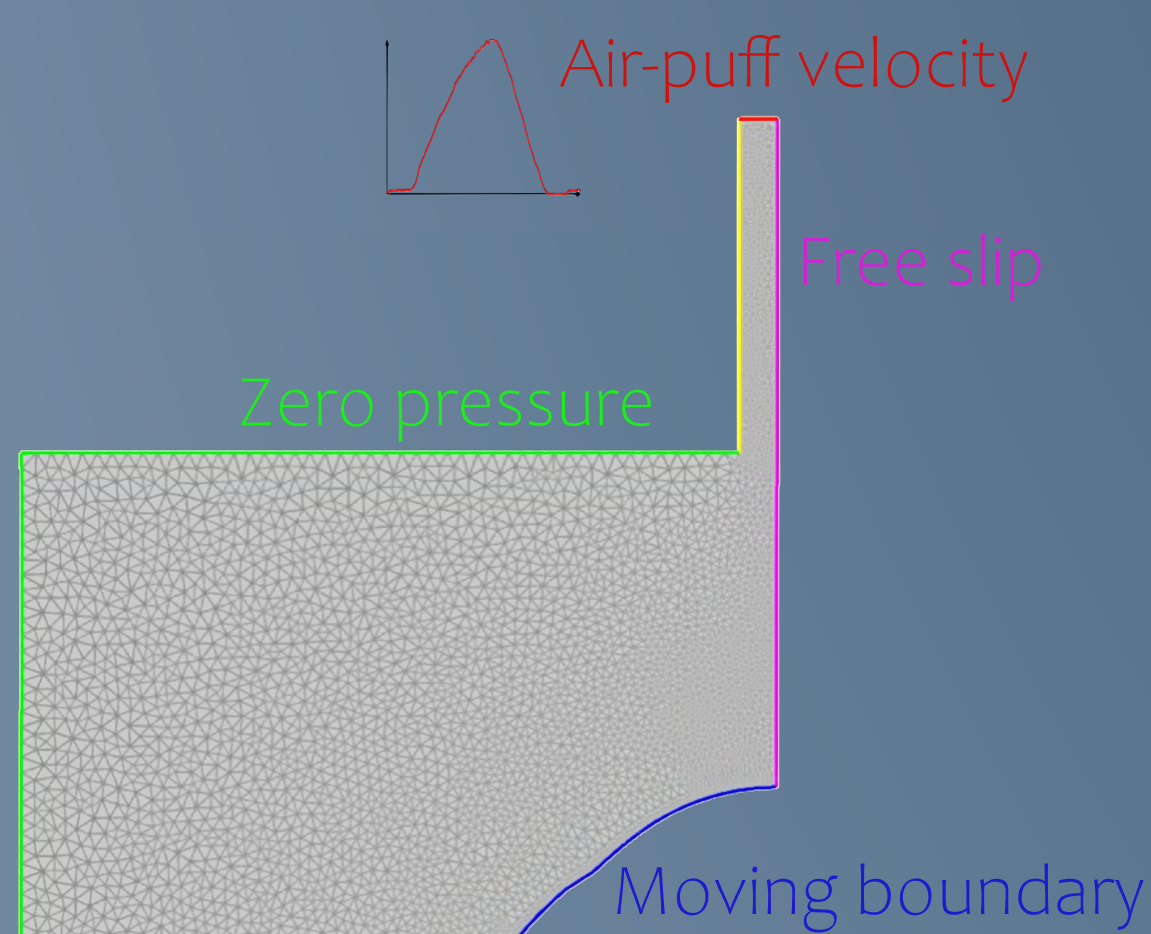


### Corneal Velocity



The **first applanation** time does not correspond to the instant of **highest velocity** of the cornea. At highest velocity, the cornea is at **equilibrium**, the net force is zero.

## CFD simulation



The **displacement** of the corneal anterior surface deriving from the **segmented images** is used to impose a **movement** to the **boundary** of the CFD simulation.

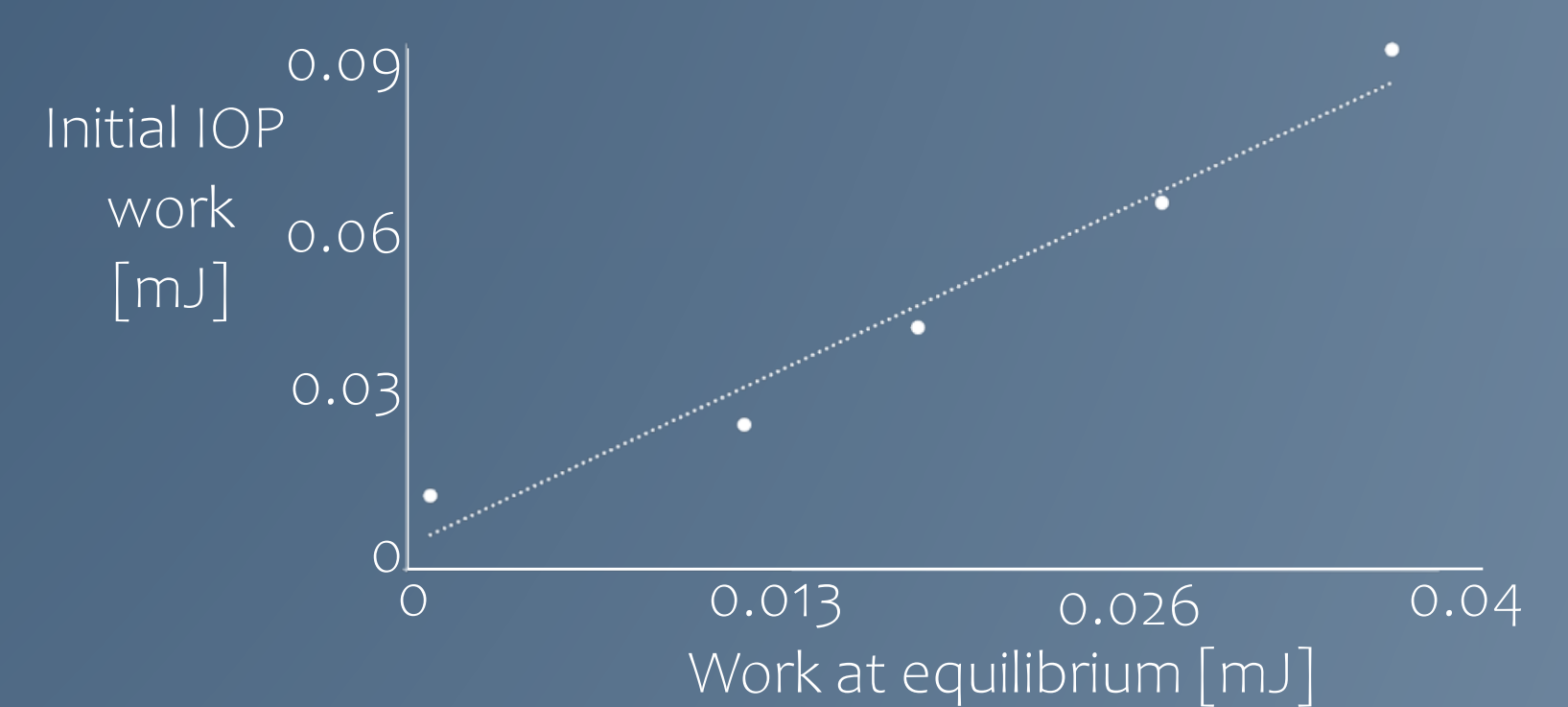
## IOP estimation

Pressure [mmHg]

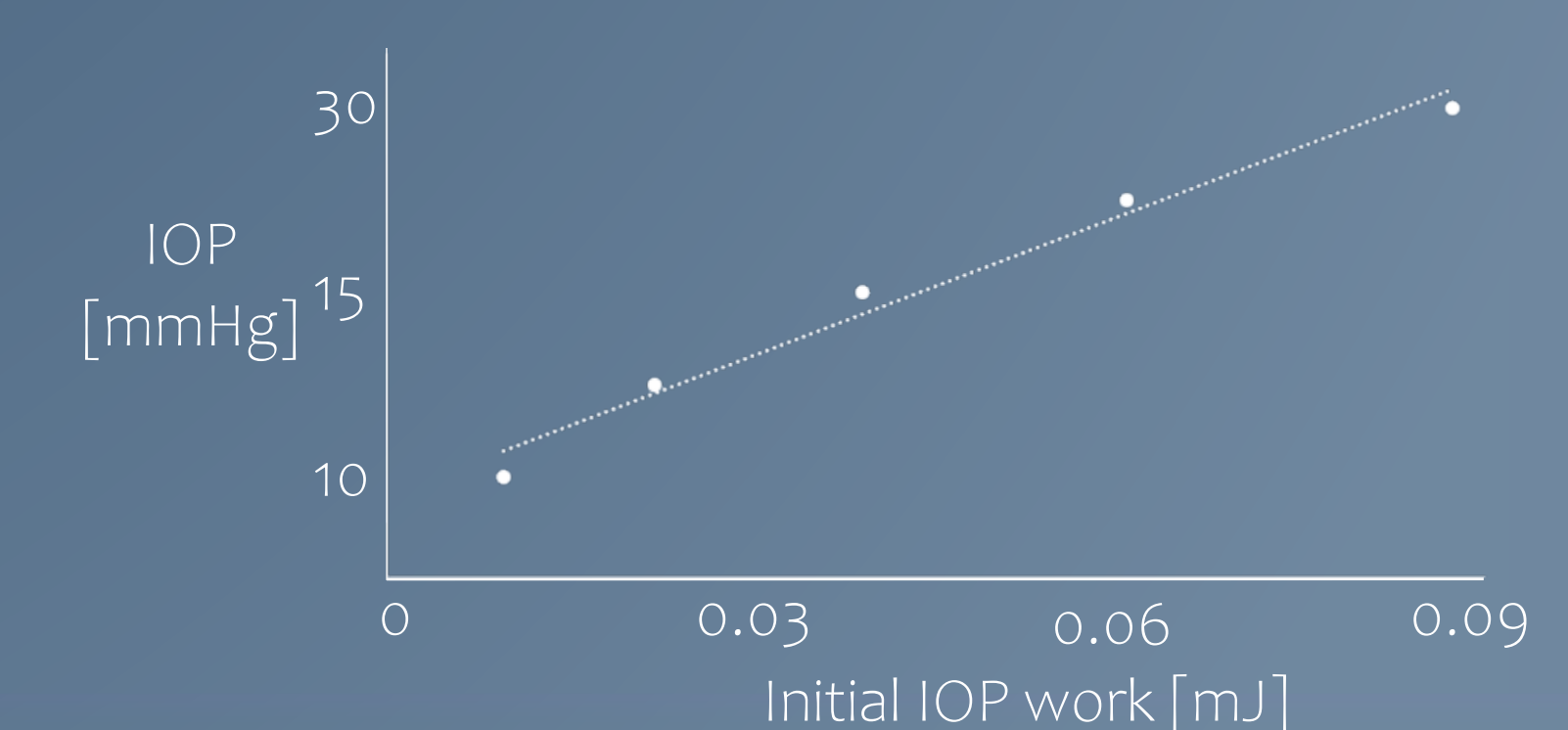


The CFD simulation gives as output the **air pressure** over the corneal surface. The pressure depends on the **movement of the eye** of the patient during the air puff.

$$\text{Initial IOP work [mJ]} = 2.1719 \cdot \text{Work at equilibrium [mJ]} + 0.0009$$



$$\text{IOP [mmHg]} = 262.56 \cdot \text{Initial IOP work [mJ]} + 8.6761$$



## Conclusions

- The equilibrium of the anterior corneal surface is considered. The mechanical properties and the thickness of the cornea does not influence the methodology.
- The FSI simulation and the subsequent CFD permit to study the air pressure over the corneal surface, that is different from the air pressure at the Corvis ST nozzle.
- Combining numerical simulations and the segmentation of clinical images it is possible to estimate the patient-specific IOP.

## References

- [1] E. Redaelli et al., "A detailed methodology to model the Non Contact Tonometry: a Fluid Structure Interaction study." Front. Bioeng. Biotechnol., vol. 10, p. 1810, 2022.
- [2] M. Á. Ariza-Gracia et al., "Fluid-structure simulation of a general non-contact tonometry. A required complexity?" Comput. Methods Appl. Mech. Eng., vol. 340, pp. 202-215, 2018.
- [3] P. Brusini et al., "How to measure intraocular pressure: an updated review of various tonometers." Journal of clinical medicine, vol. 10, no 17, p. 3860, 2021.

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